Precision of Interferometric Diffusion Coefficients in a Four-Component System Relevant to Protein Crystal Growth: Lysozyme–Tetra(ethylene glycol)–NaCl–H₂O

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We investigate the precision of Rayleigh interferometry in evaluating the nine mutual diffusion coefficients D_{ij} defining a four-component system by investigating the system lysozyme-tetra(ethylene glycol)-NaCl-H₂O. We believe our results to be the most successful experimental determination of diffusion coefficients in quaternary systems. This choice of system is motivated by its relevance to protein crystal growth. The comparison of the D_{ij} coefficients of the quaternary system and the D_{ij} coefficients from the corresponding ternary and binary systems enables us to extract some information about the hydrodynamics and thermodynamics in solutions where protein crystals grow.

I. Introduction

Optical interferometry provides the most precise methods for determining mutual diffusion coefficients in liquids.

The principal purpose of this methodological paper is to test the precision of diffusion coefficient measurements by Rayleigh interferometry in a four-component system, relevant to crystal growth. The motivation follows.

The quality of protein crystals is important for determining their X-ray structures. On the surface, diffusion, convection, and sedimentation are significant transport processes that are involved in the nucleation and growth of protein crystals; however, convection and sedimentation are detrimental. In microgravity¹ and gelled media,² the protein transport is essentially diffusive. In either case, diffusion data are particularly important for modeling the various growth processes.

Solutions used to precipitate proteins typically contain one or more other solutes, such as salts, organic solvents, and polymers. A single additional component gives a threecomponent system; two additional components give a fourcomponent system. It has been customary in protein solution studies to describe these diffusing systems by a single pseudobinary diffusion coefficient. However, the need for a reference frame (here, the volume-fixed frame) reduces the number of independent fluxes to n - 1. Therefore, an *n*-component diffusing system has $(n-1)^2$ diffusion coefficients D_{ii} , which comprise the diffusion tensor: 4 for a three-component system, 9 for a four-component system. We have found experimentally that a cross term D_{ii} ($i \neq j$) can be very large in three-component aqueous systems containing lysozyme and a single salt, and this cross term is significantly larger than both main terms D_{ii} .³⁻⁵ Consequently, the pseudo-binary approximation is quite inadequate for modeling diffusive transport in crystal growth.

In this protein context, we find that the flows of the components calculated assuming cross-term diffusion coefficients are zero (i.e., setting $D_{ij} = 0$, $i \neq j$) can differ by as much as 10%-15% from flow values calculated with actual nonzero cross terms. These differences can have a profound effect. Neglecting cross terms can lead to the erroneous conclusion that nonprotein solute concentrations are almost the same throughout the solution, including up to the crystal interface. However, including the cross-term diffusion coefficients D_{ii} in model calculations shows that there can be a variation of several percent in the nonprotein solute concentration at the crystal surface, which can change as a function of time. Such variation with time can increase precipitant concentration and affect nucleation. It can also influence water and impurity inclusion in the crystal as it grows, which can cause defects, degrading the quality of the crystal.

One technique for nucleation and crystal growth in microgravity is the free interface diffusion method, where a proteinrich solution and a precipitant-rich solution diffuse together to produce nucleation conditions and then further diffuse toward a uniform concentration distribution having slow growth conditions. Because nucleation conditions are sensitive to small concentration differences, cross-term diffusion coefficients are also important here.

For the previously described reasons, experimental diffusion studies in multicomponent protein systems have generated considerable interest. Our previous studies involved the threecomponent systems that had aqueous lysozyme (a representative protein) and a single additional component.

The group in Fort Worth, TX, has focused on threecomponent aqueous lysozyme systems with single-salt precipitants and has been supported by the National Aeronautics and Space Administration (NASA).^{3–5} The group in Naples, Italy has focused on three-component aqueous lysozyme systems with polymer additives, such as poly(ethylene glycol) (PEG) of varying molecular weights, and has been supported by ASI (the Italian Space Agency).^{6,7} Both groups have collaborated closely for many years. Because most protein precipitation protocols

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involve at least four components, it seems desirable to examine the precision of diffusion measurements for a four-component lysozyme system that contains a salt plus a PEG polymer.

Unfortunately, most polymer additives, such as PEG, are polydisperse, which already makes them multicomponent systems by themselves and, thus, considerably complicates the data analysis.^{8,9} It is possible to partially correct for polydispersity; however, accuracy is reduced.¹⁰ Therefore, we have chosen monodisperse PEG4 as the polymer additive as a way of checking our ability to make precision measurements of the D_{ij} of a four-component system. The test system chosen is lysozyme (component 1, 0.6 mM)–PEG4 (component 2, 0.5 M)–NaCl (component 3, 0.5 M)–H₂O (component 0) at pH 4.5 and 298.15 K. It represents a good example of a four-component protein-precipitant system, even though PEG4 itself is not usually used as a precipitant.

There are few published results of the nine D_{ij} diffusion coefficients for four-component systems. These include measurements by diaphragm cells^{11–13} and Taylor dispersion,^{14–16} one of which involved protein systems.¹⁶ The only previous interferometric results¹⁷ were obtained at the Naples facility by Gouy interferometry on the system cyclodextrin–phenyalanine– monobutylurea–H₂O.

The present work was done in collaboration at Texas Christian University in Forth Worth using automated Rayleigh interferometry on the Gosting diffusiometer,¹⁸ which is the world's highest precision apparatus for optical diffusion measurements. Gouy and Rayleigh measurements should give the same results in principle and are extremely similar in practice.^{19–21} However, Rayleigh interferometry is the easiest for automation, which makes many more scans possible, which, in turn, give higher precision. Furthermore, in contrast to Gouy, extraction of the D_{ij} from the Rayleigh fringe positions is more direct, and very dilute systems with few fringes can be analyzed more precisely.

We will find that the four-component Rayleigh data from the automated Gosting diffusiometer have considerably better precision than the data from the earlier four-component Naples measurements, with most D_{ij} errors being quite small. We will also see that some cross-term coefficients are large, and that D_{31} is 7 times larger than the largest of the main terms.

We will also provide some comparisons of the interesting specific effects of adding PEG4 to the ternary protein system $lysozyme-NaCl-H_2O$.

II. Data Analysis

Kim considered various possible analysis methods for obtaining the nine D_{ij} coefficients from four-component Gouy fringe pattern data in 1966 and 1969,^{22,23} one of which involved combining Rayleigh and Gouy fringe patterns. However, no actual working procedure was presented.

In 1972, Eppstein and Miller, following a suggestion by Albright, worked out the first successful analysis of Rayleigh fringes from ternary systems. It was described briefly in various papers, and in detail in ref 19. In 1973, one of us (DGM) also realized that the principles of the ternary analysis could be directly extended to four-component systems. At that time, he performed the complex algebra that related the nine D_{ij} coefficients to the nine parameters determined by nonlinear least-squares calculations from the Rayleigh fringe position measurements.

High precision in the four-component fringe positions is essential, because the uncertainties from least-squares calculations for the nine parameters of a four-component system will be larger than those for the four parameters of a three-component system. Such precision was not available to us in 1973. As a result, the four-component Rayleigh analysis procedure was put aside.

The Gosting diffusiometer¹⁸ became available to us in 1981. In 1987, it was discovered that an analysis of Gouy data could be put into a form directly analogous to the Rayleigh analysis, with the same least-squares parameters and same equations relating them to the D_{ij} coefficients. These Gouy results and the earlier Rayleigh analysis were published in 1988 for three- and four-component systems with distinct eigenvalues.²⁴ An analysis of equal eigenvalues in three- and four-component Rayleigh systems has also been presented.²⁵ The new Gouy procedure was applied to the four-component data from the diffusiometer at the Naples facility, as noted previously.¹⁷

Subsequently, the four-component Rayleigh analysis was incorporated into the automated procedure for the Gosting machine measurements. With automation, the Gosting machine's already high precision has been improved enough to get excellent values of the nine four-component D_{ij} coefficients.

The general outline of the data analysis is given in ref 24, and the relevant equations for free-diffusion boundary conditions are

$$f(j) = \frac{2j - J}{J} = \Gamma_1 \operatorname{erf}(s_1 y_j) + \Gamma_2 \operatorname{erf}(s_2 y_j) + \Gamma_1 \operatorname{erf}(s_3 y_j) \quad (1)$$

$$\Gamma_1 = a_1 \alpha_1 + a_2 \alpha_2 + a_3 \alpha_3 \tag{2}$$

$$\Gamma_2 = b_1 \alpha_1 + b_2 \alpha_2 + b_3 \alpha_3 \tag{3}$$

$$\Gamma_3 = 1 - \Gamma_1 - \Gamma_2 \tag{4}$$

where *j* is a number defining the sequence number of a fringe center in the Rayleigh pattern at a position y_j ; y_j , which is defined below, is the reduced fringe position corresponding to *j*; *J* is the total number of interference fringes (generally not an integer); and the s_i parameters are $1/\sqrt{\lambda_i}$, where λ_i are the eigenvalues of the diffusion coefficient matrix. Earlier nonautomated analysis methods used the fringe position corresponding to an integer value of *j*. Our current method uses fixed positions and associates a value *j* (now the center of a shifted fringe) to each position; these *j* values are not necessarily integers.

The α_i parameters are the refractive index fractions:

$$\alpha_i = \frac{R_i \Delta c_i}{\sum_{k=1}^3 R_k \Delta c_k}$$
(5)

The R_i parameters are the refractive index increments that best relate the total number of fringes J to the concentration differences Δc_i across the initial boundary for a given experiment according to the equation

$$J = \sum_{k=1}^{3} R_k \Delta c_k \tag{6}$$

A minimum of three experiments is required with different $\Delta c_i / \Delta c_j$ ratios to isolate the three R_i values. The values of the three R_i parameters were determined by the method of least squares by weighting the sets of J and Δc_i values from all the experiments equally.

The y_i values are the reduced fringe positions:

$$y_j = \frac{x_j - x_{J-j}}{4\sqrt{t}} \tag{7}$$

where x_j and x_{J-j} are the positions of the symmetrically paired fringes *j* and (J - j) (Creeth pairs)²⁶ and *t* is the corrected time of starting the run.²⁷ Each experiment has ~50 scans at different "clock" times, which permits this correction of the experimental clock time by a value Δt , the time from an infinitely sharp boundary to the start of the clock time. Symmetrical pairing of the fringes eliminates both a concentration dependence and a large optical aberration (Wiener skewness).²⁶ For each *j* in a given experiment, the values of y_j after time correction should be the same for each scan, so they can be averaged in preparation for the overall least-squares calculation.

The f(j) and symmetrically paired fringes are obtained as follows.

The automation procedure collects several intensities for each pixel in each horizontal scan of the 6000 vertically arranged pixels. The minimum intensity in the horizontal direction is determined for each pixel by least-squares calculation. Pixels in the top part of the fringe pattern (after baseline correction¹⁹) have a fixed horizontal minimum position, because the fringe is vertical there. This position is denoted as fringe "0". As the boundary is entered when one moves downward (i.e., with increasing x_i and y_i), the corresponding pixels show a shift of horizontal position of the minimum. This shift, divided by the interfringe distance, is a fringe shift, j. Moving further downward into the boundary, the minimum intensity position approaches the "edge" of the diffraction pattern. At this point, the minimum intensity position that is one interfringe distance back is now taken as the *position* shift for this pixel, but a value of 1 is added to the corresponding *fringe* shift. This process is repeated until the downward recording of minima is outside the boundary and into the vertical fringe in the bottom part of the pattern. The final total fringe shift is the total number of fringes, J, and the agreement of its value with that obtained by the fractionalpart-of-the-fringe measurement¹⁹ is a useful diagnostic.

At this point, there is a value of *j* for each pixel of the 6000 pixels. From them, the *reduced fringe number*, f(j) = (2j - J)/J, of eq 1 is obtained for each pixel of that scan. The values of *j* run from 0 to *J*, and those for f(j) run from -1 to +1.

Within the diffusion boundary portion of the fringe pattern, the vertical positions for a set of 100 evenly spaced f(j) values between j = 0 and j = J are obtained for each scan by curvefitting procedures. These positions and the mean time of the scan are stored for each scan. Initial solute concentrations for the experiment are also stored. These data, from three or more experiments, are recalled by a program (QFIT) and used to calculate the nine quaternary diffusion coefficients and give an estimate of their uncertainty. Separations of symmetric f(j)values are first calculated by the QFIT program,²⁷ and these are then used to calculate the quaternary diffusion coefficients.

A four-component system requires a minimum of three experiments, which must have different α_i values, or else the parameters a_i and b_i cannot be distinguished. Typically, seven experiments are used to improve statistics and check for any bad experiments. The seven sets of $\alpha_i(\alpha_1,\alpha_2,\alpha_3)$ are best chosen to be as orthogonal as possible. These correspond to A(1,0,0), B(0,1,0), C(0,0,1), D(1/2,1/2,0), E(1/2,0,1/2), F(0,1/2,1/2), and G(1/3,1/3,1/3).

The experimental quantities for each of the experiments are j, J, x_j , t, and, therefore, f(j) and y_j . The nine experimental least-

squares parameters are the three a_i values, the three b_i values, and the three s_i values of eqs 1–3. They are obtained by nonlinear least-squares calculations from the seven sets of f(j)data from the seven corresponding experiments, using the Marquardt method.²⁷ This iterative procedure requires initial values of the parameters a_i , b_i , and s_i . Suitable values, based on the assumption that $D_{ij} = 0$ (for $i \neq j$), are $(a_1 = 1, a_2 = a_3 =$ 0), $(b_2 = 1, b_1 = b_3 = 0)$, and $(s_1 = 1/\sqrt{D_1}, s_2 = 1/\sqrt{D_2}, s_3 =$ $1/\sqrt{D_3}$). The values of D_i are obtained by treating each of the three runs with $\alpha_i = 1$ as a binary.

The nonlinear least-squares procedure now follows steps 4-7 in the Analysis of Data section of ref 17.

III. Experimental Section

1. Materials. Hen egg-white lysozyme, recrystallized six times and lyophilized, was purchased from Seikagaku America and used without further purification. The molecular mass of lysozyme solute was taken to be 14 307 g mol⁻¹, and this value was used to calculate all molar concentrations, after correction for the moisture and chloride content.^{3,4} Tetra(ethylene glycol) (PEG4) was purchased from Aldrich (purity listed as 99%+) and used without further purification. The molecular mass of PEG4 solute was taken to be 194.23 g mol $^{-1}$, and this value was used to calculate all molar concentrations. NaCl was purchased from Aldrich (purity listed as 99.9%), dried by heating at 450 °C (as recommended by Rard²⁸), and used without further purification. Its molar mass was taken to be $58.443 \text{ g mol}^{-1}$, and its crystal density was taken to be 2.165 g cm⁻³, for buoyancy corrections.²⁹ Deionized water was distilled and then passed through a four-stage Millipore filter system to provide high-purity water for all the experiments. The molar mass of water was taken to be 18.015 g mol⁻¹.

2. Preparation of Solutions. All solutions were prepared by weight, using a Mettler Toledo model AT400 electro balance. The quaternary solutions used for diffusion and viscosity experiments were prepared using dry NaCl and stock solutions for both lysozyme-water and PEG4-water. A detailed description of the preparation of solutions has been described elsewhere.^{3,4}

3. Density Measurements. All density measurements were performed with a Mettler-Paar model DMA40 density meter that was thermostated with water from a large, well-regulated (± 0.01 °C) water bath. This instrument is interfaced to a computer for time averaging and gives a precision of $\pm 2 \times 10^{-5}$ g cm⁻³ or better.^{3,4}

4. Viscosity Measurements. Viscosity measurements were performed on both the binary system PEG4–H₂O and the ternary system PEG4–NaCl–H₂O, using an Ubbelhode viscometer in a bath at 25.00 \pm 0.01 °C, with the viscosity of water as a reference.³⁰

5. Free-Diffusion Measurements. The Gosting diffusiometer, used for our diffusion experiments, was designed and assembled at the Institute for Enzyme Research in Madison, WI, during the 1960s and early 1970s under the direction of Louis J. Gosting.¹⁸ It was subsequently at the University of Connecticut, then at Lawrence Livermore National Laboratory, and is now at Texas Christian University. It uses the Philpot–Cook arrangement of Rayleigh optics.³¹

The light source was a He–Ne green laser, with a wavelength of 543.5 nm in air. The automation of fringe pattern acquisition in real time with a scanner using a 6 cm photodiode array, which was designed and constructed by M. E. Zeidler, is described by Rard et al.²⁷ The principles of the Rayleigh procedure, although in terms of reading photographic plates, are detailed

TABLE 1: Individual Experiments

	А	В	С	D	Е	F	G
	$\alpha = [1,0,0]$	$\alpha = [0,1,0]$	$\alpha = [0,0,1]$	$\alpha = [1/2, 1/2, 0]$	$\alpha = [1/2, 0, 1/2]$	$\alpha = [0, 1/2, 1/2]$	$\alpha = [1/3, 1/3, 1/3]$
$\overline{c}_1 \text{ (mmol dm}^{-3}\text{)}$	0.6000	0.6000	0.6000	0.6000	0.6000	0.6000	0.6000
$\overline{c}_2 \pmod{\mathrm{dm}^{-3}}$	0.5000	0.5000	0.5000	0.5000	0.5000	0.5000	0.5000
$\overline{c}_3 \pmod{\mathrm{dm}^{-3}}$	0.5000	0.5001	0.5000	0.5000	0.5000	0.5000	0.5001
$\Delta c_1 \text{ (mmol dm}^{-3}\text{)}$	0.4000	0.0000	0.0000	0.2000	0.2000	0.0000	0.1334
$\Delta c_2 \text{ (mol dm}^{-3}\text{)}$	-0.00004	0.04818	-0.00008	0.02425	-0.00001	0.02405	0.01620
$\Delta c_3 \text{ (mol dm}^{-3}\text{)}$	0.0000	0.0000	0.1169	0.0000	0.0584	0.0584	0.0399
pH _{bot}	4.53	4.53	4.47	4.51	4.50	4.51	4.51
pH_{top}	4.52	4.50	4.51	4.50	4.52	4.49	4.52
$d_{\rm bot}$ (g cm ⁻³)	1.034856	1.034712	1.036317	1.034786	1.035579	1.035514	1.035299
$d_{\rm top}$ (g cm ⁻³)	1.033204	1.033328	1.031714	1.033244	1.032459	1.032517	1.032751
$J_{\rm meas}$	51.586	52.108	51.860	52.050	51.797	51.901	51.929
$J_{ m calc}$	51.587	52.071	51.836	52.031	51.751	51.931	52.024
Δt (s)	40	22	14	34	36	14	28
$D_{\rm A,meas} (imes 10^9 \text{ m}^2 \text{ s}^{-1})$	0.0963	0.6391	1.658	0.2011	0.2507	0.9720	0.3283
$D_{\rm A,calc} (\times 10^9 { m m}^2 { m s}^{-1})$	0.0963	0.6392	1.657	0.2013	0.2509	0.9721	0.3283

in ref 19. These include (a) baseline correction scans to correct for optical imperfections, done with bottom solution in both the diffusion and reference arms of the cell before sharpening the boundary; (b) fpf scans to determine the fractional part of the total fringe number accurately, done just after the sharpened boundary is allowed to diffuse; and (c) the 50 diffusion scans mentioned earlier. The magnification factor of the cylinder lens was 1.7602.

IV. Results

In Table 1, we report the results of the analysis of each individual experiment. In the table, \bar{c}_i (i = 1, 2, 3) represents the average concentration of each solute, and Δc_i is the difference between the initial concentration of the bottom and top solutions for each solute. We also report pH_{top} and pH_{bot}, and the densities d_{top} and d_{bot} of each prepared solution. Here, the subscripts "top" and "bot" respectively indicate the top and bottom solutions. In the same table, we list the measured total number of fringes (J_{meas}) and its calculated value (J_{calc}). The latter is obtained by fitting eq 6 to the ($J, \Delta c_1, \Delta c_2, \Delta c_3$) data of the seven experiments. The time offset Δt and both the calculated^{17,23} and extrapolated²³ values of the Rayleigh coefficient D_A are also included in the table.

Table 2 contains the results obtained by analyzing all seven experiments at the overall average concentrations $\overline{\overline{c}}_{i}$. For our small concentration differences, the densities are assumed to be linear in solute concentrations, in accordance with the following equation:

$$d = \bar{d} + H_1(c_1 - \bar{\bar{c}}_1) + H_2(c_2 - \bar{\bar{c}}_2) + H_3(c_3 - \bar{\bar{c}}_3) \quad (8)$$

The values of the parameters \overline{d} and $H_i = (\partial d/\partial c_i)_{cj, \neq i}$ were obtained by least-squares calculations from the densities of all seven pairs of solutions.

The partial molar volumes V_i were calculated from eqs 8 and 9 of ref 27. Table 2 also contains the refractive index increments R_i obtained from the previously noted eq 6 fit. The parameters a_i , b_i , and s_i (and the corresponding eigenvalues, λ_i) were obtained by least-squares calculations, using eq 1. Finally, the nine quaternary diffusion coefficients D_{ij}^Q are listed at the bottom of Table 2. The corresponding statistical error of each D_{ij} coefficient is obtained from the standard errors of the a_i , b_i , s_i , and R_i parameters by the propagation-of-error analysis.³²

1. Error Analysis. We first examine the precision of the quaternary D_{ij}^{Q} coefficient obtained by Rayleigh interferometry. We then compare the precision of these current Rayleigh

 TABLE 2: Overall System Data

parameter	value		
overall average concentration			
$\overline{\overline{c}}_1$	$0.6000 \text{ mmol } \text{dm}^{-3}$		
$\overline{\overline{c}}_2$	$0.5000 \text{ mol } \text{dm}^{-3}$		
$\bar{\bar{c}}_3$	$0.5000 \text{ mol } \text{dm}^{-3}$		
average density, \overline{d}	$1.034020 \text{ g cm}^{-3}$		
<i>H</i> parameter	1.034020 g chi		
H_1	4.121 g mol^{-1}		
H_1 H_2	$0.02904 \text{ g mol}^{-1}$		
H_3	$0.03921 \text{ g mol}^{-1}$		
partial molar volume	0.03921 g mor		
\overline{V}_1	$10210 \text{ cm}^3 \text{ mol}^{-1}$		
\overline{V}_2^1	$165.6 \text{ cm}^3 \text{ mol}^{-1}$		
$\frac{1}{\overline{V}_3}^2$	$19.28 \text{ cm}^3 \text{ mol}^{-1}$		
\overline{V}_0	$18.062 \text{ cm}^3 \text{ mol}^{-1}$		
refractive index increment			
R_1	$129000 \text{ dm}^3 \text{ mol}^{-1}$		
R_2	$1080 \text{ dm}^3 \text{ mol}^{-1}$		
$\bar{R_3}$	$444.3 \text{ dm}^3 \text{ mol}^{-1}$		
eigenvalue			
λ_1	$0.0857 \times 10^{-9} \mathrm{m^2 s^{-1}}$		
λ_2	$0.547 \times 10^{-9} \mathrm{m^2 s^{-1}}$		
λ_3	$1.18 \times 10^{-9} \mathrm{m^2 s^{-1}}$		
parameters from eq 1^a			
a_1	0.0357 ± 0.0075		
a_2	0.133 ± 0.016		
a_3	1.239 ± 0.016		
b_1	0.051 ± 0.012		
b_2	0.887 ± 0.014		
b_3	-0.219 ± 0.017		
<i>S</i> ₁	291.1 ± 1.1		
<i>s</i> ₂	427.3 ± 3.8		
<i>S</i> ₃	1080.2 ± 3.2		
quaternary coefficient			
D_{11}	$(0.08706 \pm 0.00053) \times 10^9 \mathrm{m^2 s^{-1}}$		
D_{12}	$(0.000104 \pm 0.000012) \times 10^9 \text{ m}^2 \text{ s}^{-1}$		
D_{13}	$(0.0000911 \pm 0.0000078) \times 10^9 \mathrm{m^2 s^{-1}}$		
D_{21}	$(4.00 \pm 0.56) \times 10^9 \mathrm{m^2 s^{-1}}$		
D_{22}	$(0.5633 \pm 0.0077) \times 10^9 \mathrm{m^2 s^{-1}}$		
D_{23}	$(0.0619 \pm 0.0040) \times 10^9 \text{ m}^2 \text{ s}^{-1}$		
D_{31}	$(8.1 \pm 2.1) \times 10^9 \mathrm{m^2 s^{-1}}$		
D_{32}	$(0.160 \pm 0.022) \times 10^9 \mathrm{m^2 s^{-1}}$		
D_{33}	$(1.163 \pm 0.010) \times 10^9 \mathrm{m^2 s^{-1}}$		

^a Obtained using a least-squares fit.

measurements on the Gosting machine with the earlier Gouy measurements on the machine at the Naples facility.

2. Lysozyme Systems. We observe the following, in terms of the propagation-of-errors results:

(1) Errors of the main terms D_{ii}^{Q} are ~0.5%-1.5% of D_{ii}^{Q} itself and are slightly larger than the corresponding ternary main terms D_{ii}^{T} .

TABLE 3: Comparisons of Quaternary Diffusion Coefficients of Lysozyme–Tetra(ethylene glycol)–NaCl–H₂O, Calculated Using Different Sets of Experiments

	all	all but D	all but E	all but F	all but G
		Quaternary D	Diffusion Coefficient, D_{ij} (× 1)	$10^9 \text{ m}^2 \text{ s}^{-1}$)	
D_{11}	0.08706 ± 0.00053	0.08714 ± 0.00072	0.08692 ± 0.00053	0.08698 ± 0.00056	0.08701 ± 0.00064
D_{12}	0.000104 ± 0.000012	0.000104 ± 0.000013	0.000105 ± 0.000011	0.000106 ± 0.000013	0.000103 ± 0.000014
D_{13}	0.0000911 ± 0.0000078	0.0000897 ± 0.000094	0.0000906 ± 0.0000070	0.0000901 ± 0.0000089	0.0000911 ± 0.0000091
D_{21}	4.00 ± 0.56	3.84 ± 0.82	4.16 ± 0.57	4.11 ± 0.59	4.06 ± 0.69
D_{22}	0.5633 ± 0.0077	0.5633 ± 0.0086	0.5636 ± 0.0072	0.5606 ± 0.0091	0.5638 ± 0.0090
D_{23}	0.0619 ± 0.0040	0.0623 ± 0.0047	0.0619 ± 0.0036	0.0617 ± 0.0045	0.0620 ± 0.0046
D_{31}	8.1 ± 2.1	8.8 ± 3.1	7.7 ± 2.1	7.6 ± 2.2	7.9 ± 2.5
D_{32}	0.160 ± 0.022	0.160 ± 0.025	0.159 ± 0.021	0.170 ± 0.027	0.159 ± 0.026
D_{33}	1.163 ± 0.010	1.163 ± 0.012	1.1634 ± 0.0092	1.165 ± 0.011	1.163 ± 0.012
	Refractive Index Increment, R_i (dm ³ mol ⁻¹)				
R_1	$(1.2904 \pm 0.0012) \times 10^{5}$	$(1.2900 \pm 0.0013) \times 10^{5}$	$(1.2903 \pm 0.0015) \times 10^{5}$	$(1.2903 \pm 0.0014) \times 10^{5}$	$(1.29084 \pm 0.00075) \times 10^{5}$
R_2	$(1.0803 \pm 0.0010) \times 10^3$	$(1.0805 \pm 0.0011) \times 10^3$	$(1.0802 \pm 0.0012) \times 10^3$	$(1.0806 \pm 0.0012) \times 10^3$	$(1.08066 \pm 0.00062) \times 10^3$
R_3	444.27 ± 0.42	444.12 ± 0.47	444.27 ± 0.42	444.30 ± 0.49	444.41 ± 0.26

(2) The largest errors are in those cross-term diffusion coefficients D_{ij}^Q ($i \neq j$) that correspond to the motion of small solutes, because of the concentration gradient of the largest ones. This same behavior is found in the ternary systems.^{3,33}

(3) The errors in these quaternary cross-term coefficients are always larger than the analogous ones from the corresponding ternaries.^{3,33} They can also reach ~25% of D_{ij}^{Q} . We also observe large errors in the cross-term coefficients for the motion of the largest molecule (lysozyme), because of the concentration gradients of the small ones. This probably depends on numerical problems that are encountered in obtaining the very small values of these coefficients.

3. Comparison with the Earlier Four-Component System. For a proper comparison of our Rayleigh results with the earlier Gouy interferometric four-component system of cyclodextrin– phenylalanine–monobutylurea– H_2O , we must use the same method of estimating the errors.

When the Gouy system was analyzed in 1992,¹⁷ the propagation-of-error equations, which include 93 nonzero derivatives, had not yet been derived. Consequently, the precision of each D_{ij} coefficient was estimated as follows. Data for one or more experiments, in turn, were deleted, always keeping the three α_i = 1 cases.^{17,20} The D_{ij} coefficients were then calculated for each set by the previously described nonlinear least-squares procedure. There were six such sets, including the set of all eight experiments. The estimated error for each D_{ij} coefficient was taken as the standard error of the mean of its values from the six sets.

A similar analysis of our current Rayleigh results was obtained by removing, one at a time, the following data sets from the full set of seven, keeping the three $\alpha_i = 1$ cases, as was done with the Gouy data: D(1/2, 1/2, 0), E(1/2, 0, 1/2), F(0, 1/2, 1/2), or G(1/3, 1/3, 1/3), where the parentheses contain the α_i values. The results from these four cases, plus the full set of seven, are given in Table 3.

Table 3 shows that, for each D_{ij}^Q coefficient, the differences between its value for the complete set of seven experiments and its values from each of the four six-experiment sets are always within one standard deviation of the complete set. Moreover, these differences are generally very small, except for D_{21}^Q and D_{31}^Q and, in one case, for D_{32}^Q (the "all but F" case). In these cases, the differences are as follows: 1.5%-4% for D_{21}^Q , with a corresponding relative standard error of 14%; 2.5%-8% for D_{31}^Q , with a corresponding relative standard error of 14%. These relative standard errors are found in Table 4; they are denoted by %SE, are equal to $100 \times$ (the standard error from propagation of error equations)/ D_{ij}^{Q} , and are based on the complete set.

These results confirm the general rule that the largest variations are observed for the cross-term diffusion coefficients D_{ij}^{Q} for which the ratio R_j/R_i is larger than unity. The R_i parameter and the ratios R_j/R_i are in Table 4, as are the eigenvalues λ_i . We also observe that the D_{ij}^{Q} errors do not increase much in going from seven to six experiments.

Some idea of the improved precision from the Gosting diffusiometer for four-component systems may now be obtained from a comparison with the earlier Gouy results.¹⁷ Table 4 contains, for each of the nine D_{ij}^{Q} coefficients, the standard error of the mean of its values from all six sets of Gouy experiments for cyclodextrin—phenyalanine—monobutylurea— H_2O and the percentage relative standard deviation of the corresponding mean for this system.¹⁷ Our corresponding Rayleigh results from the Gosting machine for lysozyme—tetra-(ethylene glycol)—NaCl— H_2O are also included, as well as the propagation-of-error and relative propagation-of-error results. We note that that the standard-error-of-the-mean results are significantly smaller than the propagation-of-error results. This implies a very consistent series of experiments.

The error comparison for the two systems is based on a common treatment of the data, namely, averaging the D_{ii}^Q coefficients from various combinations of experiment sets and calculating the standard deviation of the mean. It cannot really be completely correct because the two systems are different, and relative values of the D_{ij} , λ_i , and R_i can significantly influence the least-squares fitting errors. In particular, the mainterm errors depend on D_{ij} and λ_i , and the cross-term errors depend on D_{ij} , λ_i , and R_i . When the ratio R_j/R_i is large, errors in the D_{ij} are also large.¹⁷ Furthermore, convergence is better and errors are smaller when the eigenvalues λ_i are significantly different. This is the case here but is not so for the earlier Gouy system, where λ_2 and λ_3 are very close (cf. Table 4). Finally, the differing difficulties of solution preparation also contribute to differences in errors. Nonetheless, the percentage relative errors from the Gosting-machine Rayleigh results are significantly smaller than those for the Gouy results. This is particularly true for the cross terms, even though the ratios R_1/R_2 and R_1/R_3 are considerably larger than those for the earlier Gouy system. This suggests that the automated Gosting diffusiometer and its Rayleigh procedures have significantly improved the relative precision of determining the cross terms and probably all terms.

TABLE 4: Comparison of Four-Component D_{ij} (10⁹ m² s⁻¹) Errors on the Same Basis^a

	CD-PA-MBU-H ₂ O ^b			lysozyme-PEG4-NaCl-H ₂ O				
	D_{ij}	SD mean	%SD mean	D _{ij}	SD mean	%SD mean	SE from POE	%SE
D_{11}	0.316	0.001	0.32	0.0871	0.00009	0.10	0.00053	0.61
D_{12}	-0.001	0.001	100.0	0.00010	$9. \times 10^{-7}$	0.91	1.16×10^{-5}	110.2
D_{13}	-0.001	0.0001	10.0	0.000091	$6. \times 10^{-7}$	0.678	$0.78 imes 10^{-5}$	8.6
D_{21}	-0.132	0.030	22.7	4.004	0.124	3.10	0.561	14.0
D_{22}	0.646	0.013	2.0	0.563	0.0013	0.232	0.0077	1.37
D_{23}	0.064	0.003	4.7	0.0619	0.00021	0.339	0.00403	6.51
D_{31}	-0.076	0.061	80.3	8.104	0.465	5.74	2.05	25.1
D_{32}	0.001	0.021	2100	0.1603	0.0047	2.94	0.0225	14.02
D_{33}	0.632	0.003	0.47	1.163	0.00074	0.064	0.0102	0.88
λ_1	0.3151			0.0851				
λ_2	0.6294			0.5477				
λ_3^-	0.6492			1.1801				
R_1	139.5			129045				
R_1	36.51			1080				
R_3	17.30			444.3				
R_1/R_2	3.8			119.5				
R_1/R_3	8.1			290.4				
R_2/R_3	2.1			2.4				

^{*a*} D_{ij} are the coefficient values from all the experiments. SD mean is the standard error of the mean; %SD mean is $100 \times (\text{SD mean})/D_{ij}$. SE from POE is the standard error of the coefficient from the propagation-of-error calculation; %SE is $100 \times (\text{SE from POE})/D_{ij}$. Units of all D_{ij} and λ_i are $10^9 \text{ m}^2 \text{ s}^{-1}$. ^{*b*} α -cyclodextrin–L-phenylalanine–monobutylurea–H₂O.¹⁴

V. Discussion of Diffusion Coefficients

The superscripts Q (quaternary), T (ternary), and B (binary), where $D_{ii}^{B} = D_{i}$, have been used to distinguish the various coefficients in the following discussion.

It is possible to envision the properties of the diffusion coefficients in terms of viscosity, electrostatic, obstruction, and excluded volume effects. The mixing of these macroscopic and microscopic concepts is not exact. For example, a direct connection between viscosity and diffusion is forbidden by the "Curie principle" of irreversible thermodynamics, because they are of different tensor orders.^{34–36} However, these concepts often provide a useful picture and qualitative approximations of the four-component quantities, on the basis of binary or ternary data, as will be seen below.

1. Quaternary Diffusion Coefficients. In Table 2, we observe the following, for the cross-term diffusion coefficients: (1) All the cross-term diffusion coefficients are positive.

(2) The D_{12}^{Q} and D_{13}^{Q} values are very small (between 10^{-13} and 10^{-14} m² s⁻¹).

(3) The D_{23}^{Q} and D_{32}^{Q} values are small (between 10^{-10} and 10^{-11} m² s⁻¹).

(4) The D_{21}^{Q} and D_{31}^{Q} values are quite large ($\sim 5 \times 10^{-9}$ m² s⁻¹), and both are larger than all the main-term diffusion coefficients.

The corresponding ternary system without PEG4 exhibits similar behavior:³ D_{13}^{T} is very small, D_{31}^{T} is very large, and D_{31}^{T} is larger than both main-term diffusion coefficients D_{11}^{T} and D_{33}^{T} .

On the basis of published and unpublished data for several similar three- and four-component systems, cross-term diffusion coefficients for the motion of a large molecule due to the concentration gradient of a much smaller one are almost negligible. On the other hand, cross-term diffusion coefficients for the motion of a small molecule due to the concentration gradient of a much bigger one can be quite large. In intermediate cases, cross-term diffusion coefficients increase as the difference in size of the two solutes increases.^{37–40} This behavior is essentially due to an excluded volume effect of the large molecule on the small one,^{37–38} combined with the choice of

the molar concentration scale that does not take into account the big difference in the solute molecular weight.

2. Effect of PEG4 on Lysozyme–NaCl Coupled Transport. We now consider the effects of PEG4 on the diffusion coefficients D_{11}^Q , D_{33}^Q , D_{13}^Q , and D_{31}^Q .

2.1. D_{11}^Q . The value of the D_{11}^Q coefficient is (0.0870 \pm 0.0005) $\times 10^{-9}$ m² s⁻¹. The ternary diffusion coefficient for the system lysozyme(1)-NaCl(3)-H₂O is $D_{11}^T = (0.1182 \pm 0.0005) \times 10^{-9}$ m² s⁻¹, whereas the corresponding binary diffusion coefficient for lysozyme(1)-water is $D_{11}^B = 0.5508 \times 10^{-9}$ m² s⁻¹.³

The dramatic decrease from the value of D_{11}^{B} to the value of D_{11}^{T} is a consequence of the electrostatic coupling of the motions between ionic species. The diffusion coefficient of electrolytes in aqueous binary systems depends on the diffusivities (mobilities) of both ions and their electrostatic interaction. Because the ions are not independent of each other, the faster ion speeds up the slower one; conversely, the slower ion slows down the faster one. The experimental diffusion coefficients of the salt is then a combination of the interconnected diffusivities of both ions.³

This same situation also occurs in binary aqueous solutions of polyelectrolytes or charged proteins. The only difference is that, in this case, the number z_p of low-molecular-weight dragging ions (the counterions) is large. Furthermore, the difference between the diffusivity of the charged protein and its counterions is also large, with the protein diffusivity being much smaller. However, adding NaCl to the protein solution decreases the electrostatic potential between the polyions and the counterions, so the dragging effect also decreases. Consequently, D_{11}^{T} is more similar to the value of the protein diffusivity by itself, and, thus, is much smaller than the D_{11}^{B} value.

The decrease from the values of D_{11}^{T} to the value of D_{11}^{Q} can be simply interpreted as a consequence of an increase of the solution viscosity from the added PEG4.^{33,39} This is predicted by the Stokes–Einstein equation applied to microscopic systems. Indeed, the ratio between the lysozyme main diffusion coefficient in the presence and absence of PEG is $D_{11}^{Q}/D_{11}^{T} = 0.736$ ± 0.007 , whereas the inverse ratio of the corresponding

TABLE 5:	Diffusion	and	Viscosity	Ratios
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diffusion ratio	viscosity ratio				
Component 1					
$D_{11}^{\rm Q}/D_{11}^{\rm T} = 0.736 \pm 0.007$	$1/(\eta^{\rm Q}/\eta^{\rm T}) = 0.752 \pm 0.008$				
$D_{11}^{\rm T}/D_{11}^{\rm B} = 0.215 \pm 0.001$	$1/(\eta^{\mathrm{T}}/\eta_{1}^{\mathrm{B}}) = 0.972 \pm 0.003$				
$D_{11}^{\rm Q}/D_{11}^{\rm B} = 0.158 \pm 0.001$	$1/(\eta^{\rm Q}/\eta^{\rm B}_1) = 0.682 \pm 0.005$				
Component 3					
$D_{33}^{\rm Q}/D_{33}^{\rm T} = 0.797 \pm 0.007$	$1/(\eta^{\rm Q}/\eta^{\rm T}) = 0.752 \pm 0.008$				
$D_{33}^{\mathrm{T}}/D_{33}^{\mathrm{B}} = 0.980 \pm 0.001$	$1/(\eta^{\mathrm{T}}/\eta_{3}^{\mathrm{B}}) = 0.977 \pm 0.002$				
$D_{33}^{\rm Q}/D_{33}^{\rm B} = 0.787 \pm 0.001$	$1/(\eta^{\rm Q}/\eta^{\rm B}_3) = 0.734 \pm 0.010$				
Component 2					
$D_{22}^{\rm Q}/D_{22}^{\rm B} = 0.932 \pm 0.014$	$1/(\eta^{\rm Q}/\eta^{\rm B}_2) = 0.952 \pm 0.006$				

viscosities is similar, with $\eta^{\rm T}/\eta^{\rm Q} = 0.752 \pm 0.008$. (See Table 5.) Here, the Stokes-Einstein equation is quite successful in solutions with a relatively low concentration of macromolecules. This strong correlation between diffusion and viscosity is generally observable when the diffusing species (i.e., the protein) is large, with respect to those other components of the system (i.e., H₂O, NaCl, and PEG4) that can be approximated as a continuum. However, when electrostatic coupling occurs, viscosity poorly correlates with diffusion, and the difference between $D_{11}^{\rm B}$ and $D_{11}^{\rm T}$ cannot be predicted from the viscosity behavior.

2.2. D_{33}^Q . The value of the D_{33}^Q coefficient is $(1.16 \pm 0.01) \times 10^{-9} \text{ m}^2 \text{ s}^{-1}$. The ternary diffusion coefficient for the system lysozyme(1)-NaCl(3)-H₂O is $D_{33}^T = (1.445 \pm 0.001) \times 10^{-9} \text{ m}^2 \text{ s}^{-1}$, whereas the corresponding binary diffusion coefficient for NaCl(3)-H₂O is $D_{33}^B = 1.4740 \times 10^{-9} \text{ m}^2 \text{ s}^{-1.41}$.

The small decrease of the NaCl main-term diffusion coefficient observed by adding lysozyme to NaCl(3)–H₂O can be explained by a lysozyme obstruction effect. This effect is very small, because the lysozyme concentration is small. The further decrease of $D_{33}^{\rm T}$ to $D_{33}^{\rm Q}$ on adding PEG4 to the ternary lysozyme(1)–NaCl(3)–H₂O system may be related to a PEG obstruction effect on the motion of the simple salt. This further decrease is larger because the volume fraction occupied by PEG4 in solution is larger than that of lysozyme (the volume fraction Φ_i ($\Phi_i = c_i V_i$, with V_i given in dm³ mol⁻¹) for PEG4 is $\Phi_{\rm PEG4} \approx 0.1$ and for lysozyme is $\Phi_{\rm lys} \approx 0.01$). Here, the viscosity quantitatively fails to predict the change of this diffusion coefficient. This is not a surprise, considering the small size of both the Na⁺ and Cl⁻ ions (i.e., the continuum approximation fails).

2.3. D_{I3}^Q The quaternary D_{13}^Q coefficient, which is equal to $(0.0000911 \pm 0.000078) \times 10^{-9} \text{ m}^2 \text{ s}^{-1}$, is smaller than the corresponding ternary D_{13}^T ($D_{13}^T = (0.0001070 \pm 0.000002) \times 10^{-9} \text{ m}^2 \text{ s}^{-1}$). This cross-term diffusion coefficient is proportional to the protein mobility; therefore, we compare the ratio between it in the presence and absence of PEG4, $D_{13}^Q/D_{13}^T = 0.85 \pm 0.09$, with the inverse ratio of the corresponding viscosities, $\eta^T/\eta^Q = 0.752 \pm 0.008$. Again, the behavior of diffusion and viscosity are in reasonable agreement and within the experimental error.

2.4. D_{31}^Q . The quaternary D_{31}^Q coefficient, which is equal to $(8.1 \pm 2.1) \times 10^{-9} \text{ m}^2 \text{ s}^{-1}$, is smaller than the corresponding ternary $D_{31}^T (D_{31}^T = (13.8 \pm 0.2) \times 10^{-9} \text{ m}^2 \text{ s}^{-1})$.³ Therefore, adding PEG4 seems to decrease the effect of a lysozyme concentration gradient on the motion of the simple salt. This does not seem to strictly depend on the variation of the NaCl main-term diffusion coefficient. In fact, we have $D_{31}^Q/D_{33}^Q = 7.0 \pm 1.9$, whereas $D_{31}^T/D_{33}^T = 9.6 \pm 0.2$.

The number of NaCl molecules moved by a single lysozyme molecule also reflects this effect. This value can be obtained as follows. If we write the flux equation for both lysozyme and NaCl, we have

$$\begin{cases} J_{1}^{Q} = -D_{11}^{Q} \nabla c_{1} - D_{12}^{Q} \nabla c_{2} - D_{13}^{Q} \nabla c_{3} \\ J_{3}^{Q} = -D_{31}^{Q} \nabla c_{1} - D_{32}^{Q} \nabla c_{2} - D_{33}^{Q} \nabla c_{3} \end{cases}$$
(9)

In the absence of PEG4 and NaCl concentration gradients, eq 9 reduces to

$$\begin{cases} J_{1}^{Q} = -D_{11}^{Q} \nabla c_{1} \\ J_{3}^{Q} = -D_{31}^{Q} \nabla c_{1} \end{cases}$$
(10)

and then $J_{3/}^Q/J_1^Q = D_{31}^Q/D_{11}^Q$. This shows that the flux of NaCl per unit flux of lysozyme equals the ratio of the cross-term diffusion coefficient of NaCl, because of the lysozyme concentration gradient and the lysozyme main-term diffusion coefficient. The values of this ratio obtained for the quaternary and ternary systems are, respectively, $D_{31}^Q/D_{11}^Q = 93 \pm 25$ and $D_{31}^T/D_{11}^T = 117.2 \pm 2$, with a modest decrease for the quaternary of the number of NaCl molecules moved by lysozyme. This diffusion coefficient is the largest one, both in ternary^{3,33} and quaternary systems, and indicates the large effect of the protein molecule on the motion of the simple salt. The physical reason for such a large effect is the exclusion of the salt ions from the volume occupied by the protein, because of hard core repulsive force, as first proposed in ref 3 and later formalized in predictive equations.^{37,42}

3. Coupled Transport Directly Related to PEG4. We now analyze the quaternary diffusion coefficient related directly to the motion of PEG4.

3.1. D_{22}^Q . The value of the D_{22}^Q coefficient is $(0.563 \pm 0.008) \times 10^{-9} \text{ m}^2 \text{ s}^{-1}$, whereas the corresponding binary diffusion coefficient of PEG4(2)–H₂O is $D_{22}^B = 0.6042 \times 10^{-9} \text{ m}^2 \text{ s}^{-1.43}$ The protein volume fraction is relatively low, and electrostatic coupling does not occur; therefore, we expect that the effect of protein on the main diffusion coefficient D_{22}^Q is not significant. We also expect that the effect of the smaller NaCl on PEG4 transport is essentially related to viscosity.³³ The prediction of D_{22}^Q from D_{22}^B , using the corresponding viscosities,³⁹ is fairly good.

3.2. Other Cross-Term Diffusion Coefficients. The quaternary $D_{21}^{\rm Q}$ coefficient, although smaller than the $D_{31}^{\rm Q}$ coefficient, is large and of the same order of magnitude. The ratio $D_{21}^{\rm Q}/D_{11}^{\rm Q} = 46.0 \pm 7.2$, which indicates that substantial amounts of PEG4 are moved by a single lysozyme molecule, just as NaCl was.

However, the most interesting thing is the analysis of the ratios D_{i1}^Q/D_{ii}^Q . In fact, these ratios are very similar for PEG4 and NaCl: $D_{21}^Q/D_{22}^Q = 7.1 \pm 1.2$ and $D_{31}^Q/D_{33}^Q = 7.0 \pm 1.9$. This implies that, besides the different nature of the two solutes, the effect of lysozyme on both their motions is exactly the same. This is possible only for a nonspecific effect, such as the excluded volume effect.

4. Comments on Cross-Term Effects. When considering the magnitudes of the diffusion coefficients, we are also interested in differences in the flows with and without the cross terms. As noted in the Introduction, cross terms can have a significant effect on the nucleation and crystal growth of proteins, because these processes are sensitive to small concentration differences.

Depending on the gradients, the large values of D_{21} and D_{31} typically result in flow differences of ~10%-15%, compared to setting them equal to zero. Clearly, the nonzero cross terms do not permit a constant gradient of nonprotein solutes to remain, even if they start out that way.^{44,45} The time-dependent transport of noticeable amounts of PEG4 and NaCl by a lysozyme gradient can involve inclusion of nonprotein solutes and water in the protein crystal, alter the nucleation and precipitation processes and rates, create stress in the crystal, and degrade crystal quality.

VI. Conclusions

Rayleigh interferometry has been successfully applied for the first time to determine precision mutual diffusion coefficients in quaternary systems, using an instrument that was designed and assembled by Gosting and co-workers¹⁸ and automated by M. Zeidler and some of the current authors (JGA and DGM).²⁷ The precision of the experimental apparatus and the data processing is tested using the quaternary system lysozyme–tetra(ethylene glycol)–NaCl–H₂O. Several assessments of the quality and statistics were used to examine the data processing and precision of the apparatus. The precision seems significantly better than that from the earlier interferometric study.¹⁷

The system investigated is of interest in the field of protein crystal growth, because lysozyme is a model protein in crystallogenesis and poly(ethylene glycol) (PEG) and NaCl are widely used as crystallizing agents. The comparison of these high-precision diffusion results for this quaternary system, along with its corresponding ternary^{3,33} and binary systems,^{3,28,43} has provided information on the effect of adding PEG to protein-salt systems. The excluded volume effect and viscosity seem to be the most significant contributions to the action of PEG, although dielectric effects cannot be neglected.

The significant effects of large cross terms indicate that crystallization modeling using a pseudo-binary protein diffusion coefficient can lead to seriously misleading results.

The investigated system contains a monodisperse PEG oligomer, whereas polydisperse PEG oligomers are typically used in crystallization kits. Therefore, the present analysis will be extended to analogous protein systems containing PEG at higher molecular weights, which are polydisperse but will still have a narrow distribution of diffusion coefficients, as a function of the molecular weight.

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